One-Step Construction of Thick Multilayered Tissues by Fabrication of Layer-by-layer Nanofilms onto Ce A. Nishiguchi, H. Yoshida, M. Matsusaki, A and M. Akashi M. Matsusaki, A and M. Matsusaki, A and M. Akashi M. Matsusaki, A and M. Matsusaki, A and M. Akashi M. Matsusaki, A and M. Akashi M. Matsusaki, A and M. Matsusaki, A

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Statement of purpose: In vitro construction of layered tissues has attracted much attention in tissue engi neering. Up to date, cell sheet engineering and magnetic lip osome have been employed for layered tissue construction, but these methods can't control the thickness of extrac ellular matrix (ECM) and three-dimensional (3D) configurati on of cells. Recently, we reported hierarchical cell manipulation technique by fabrication of fibronecti n and gelatin (FN-G) nanofilms onto cell surfaces by the laverby-layer (LbL) assembly. 1) The 6 nm of FN-G nanofilms on the surface of the first layer of cells provided a suitable cell adhesive surface that is similar to the natura 1 ECM for the second layer of cells.²⁾ We successfully prepared 3Dblood vessel constructs³⁾ and clarified the effect of 3Dstructures on cellular functions. 4) Although this method was effective to control cell types one by one in t he obtained 3D-layered tissues, it had a limitation fo r a maximum layer of two-layers per day due to waiting for stable cell adhesion. For example, development of t enlayered (10L-) constructs required for at least fiv e days. To fabricate thicker 3D-tissues in one step, we dev eloped a novel one-step fabrication technology of approxim ately 10L-tissues by LbL assembly. By preparing FN-G nanofilms on a dispersed single cell surface and subsequent incubation in a cell culture insert, 3Dtissues with seven or eight layers were obtained after 24 h ours of culture (Figure 1a). Furthermore, cellular configur ation was easily controlled in the obtained tissues. This approach can be an innovative technique for tissue engineering.

Methods: The 5 x 10⁶ cells/mL human dermal fibroblast cells (hFCs) were alternatively incubated with 0.2 mg/mL FN $(M_w = 4.6 \times 10^5)$ and G $(M_w = 1.0 \times 10^5)$ in 50 mM Tris-HCl (pH = 7.4) for 1 min at 30 rpm. After repe ating the nine steps of immersion, the (FN/G)₄FN films with 6 nm thickness were prepared on the cell surface. The preparation of FN-G films onto the cell surface was confirmed by confocal laser scanning microscopic (CLSM) observation using rhodamine (Rh)-FN and FITC cells G. Moreover, the viability and proliferation of the coated with FN-G and other LbL films were also evaluated. Finally, the hFCs coated with FN-G nanof ilms were seeded into a cell culture insert and cultured for 24 or 48h to construct multilayered tissues in one ste Results: Fluorescence microscopic observations showed successful preparation of Rh-FN-FITC-G films onto t surfaces of fibroblast cells. The obtained cells wi th FN-G films onto their surface maintained high viability (> 98 %) and proliferative property. On the other hand, othe polyelectrolyte nanofilms such as FN-ε-poly(lysine) (ε-Lys) and ε-Lys-Poly(styrene sulfate sodium salt) (PSS) showed cytotoxicity depending on their thickness be cause of the condensation and strong adsorption of the ca tionic components onto the cell surface even using biocompatible FN as a counterpart component. Due to

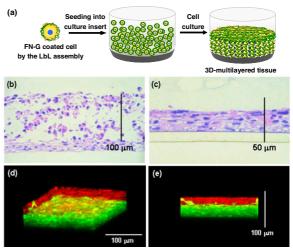


Figure 1. (a) Schematic illustration of 3D-multilay ered hFC tissues by preparing FN-G nanofilms onto single cell surface. (b, c) HE staining images of the obta architectures composed of (b) non-coated cells and (c) FN-G coated cells. (d, e) 3D-reconstructed CLSM crossection images of multilayers composed of FN-G coated cells labeled with cell tracker green and red, respectively.

binding domain interaction of negatively charged FN and G, the FN-G films did not show any cytotoxicity. 1 Hematoxylin and eosin (HE) staining and CLSM images showed the successful construction of 3D-layered architectures composed of the hFCs. Although non-co ated cells poorly adhered and layered tissues could not be constructed, FN-G coated cells indicated well adhes ion and organization and seven or eight layers were constructed in one step due to adhesive property of the FN-G nanofilms (Figure 1b, c). By repeating seeding of the hFCs stained with cell tracker green and red, e ightlayered tissues consisting of distinct two types of four layers were successfully obtained within 2 days. Conclusions: One-step construction of multilayered tissues was achieved by fabrication of FN-G nanofil ms on single cell surface within 1 or 2 days. This method ology will be useful as a build-up technique for tissue engineering.

Acknowledgement: This work was supported by an Industrial Technology Research Grant Program in 200 (06B44017a) from NEDO of Japan and PRESTO-JST.

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