

## Biomimetic Aggrecan Based on a Polyacrylic Acid (PAA) Core and Chondroitin Sulfate (CS) Bristles

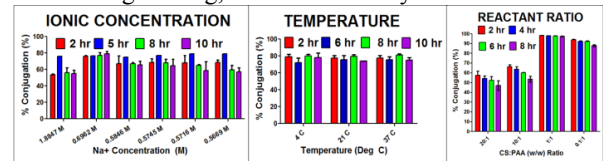
Nandita Ganesh<sup>1</sup>, Sumona Sarkar<sup>1</sup>, Dr. Ed Vresilovic<sup>2</sup>, Dr. Michele Marcolongo<sup>3</sup>

<sup>1</sup>Biomedical Engineering, Science and Health Systems, Drexel University, <sup>2</sup>Penn State Hershey Medical Center, Orthopaedic Surgery, <sup>3</sup>College of Engineering, Material Science and Engineering, Drexel University

**Statement of Purpose:** Intervertebral disc (IVD) degeneration is characterized by the loss of the proteoglycan (PG) aggrecan from the inner nucleus pulposus of the disc, which is responsible for hydration and load bearing<sup>1</sup>. Aggrecan consists of a core protein with covalently attached chondroitin sulfate (CS) chains, containing highly charged anionic groups<sup>1</sup>, which provide electrostatic repulsion and draw water into the tissue to resist mechanical deformation during loading. There is a linear reduction of aggrecan with increased degeneration<sup>2</sup> due to enzymatic cleavage of the protein core<sup>1</sup>. *The goal of the project was the fabrication of an enzymatically resistant biomimetic aggrecan brush structure (using a synthetic protein core) to serve as a minimally invasive injection procedure for the alleviation of back pain.* A biomimetic polymer was synthesized with a synthetic core protein of PAA and bio-based bristles of CS via the “grafting-to” polymerization technique.

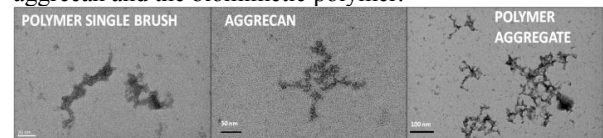
**Methods:** *Synthesis and Optimization of Reaction Conditions.* A primary amine on the terminal end of the CS (CS-4, MW 22 kDa, Sigma) was used as a handle<sup>2</sup> to conjugate it with the carboxylic acid groups present on PAA (MW 250 kDa, Sigma). PAA was activated in MES buffer using the zero length crosslinkers EDC (1-Ethyl-3-(3-dimethylaminopropyl) carbodiimide) and NHS (N-Hydroxysuccinimide) and reacted with CS in PBS buffer at pH 7.0. Reaction completeness was measured via the fluorescamine dye assay. The reaction of fluorescamine with free primary amines forms a fluorescent derivative, whose signal can be measured. Percent conjugation was calculated by normalizing the fluorescence of the conjugate against a CS control. The reaction parameters optimized were ionic concentration of buffer, temperature and reactant ratios. *Characterization.* The biomimetic polymer’s morphology was characterized by Transmission Electron Microscopy (TEM, uranyl acetate staining). Rheological measurements of solutions of CS, PAA, and polymer with PBS buffer as a control solution were conducted. (AR 2000ex rheometer, 25°C, shear rate 10-500 s<sup>-1</sup>).

**Results:** *Synthesis and Optimization of Reaction Conditions.* The ionic concentration of the buffer mixture was varied based on Na<sup>+</sup> concentrations and ~0.69 M Na<sup>+</sup> showed the highest and most consistent percent conjugation over the time of the study, thereby being considered optimal. Three reaction temperatures were investigated: 4°C, 21°C, 37°C. There was no statistically significant difference in the percent conjugation obtained, therefore 21°C was chosen as the optimal reaction temperature for convenience of lab conditions. The reactant ratios (CS:PAA, w/w) tested were 20:1, 10:1, 1:1 and 0.1:1. The 1:1 CS:PAA reached ~98% conjugation and was chosen as the optimal ratio.



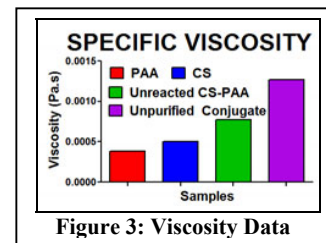
**Figure 1: Effects of Reaction Conditions**

*Characterization.* The morphology of the conjugate was characterized by TEM using aggrecan as a control. Morphological similarities were observed between the aggrecan and the biomimetic polymer.



**Figure 2: TEM Images of Aggrecan and Polymer**

Specific viscosities were calculated by normalizing sample viscosity against PBS viscosity values. The biomimetic polymer showed higher specific viscosity than CS, PAA and the mixture of unreacted CS-PAA.



**Figure 3: Viscosity Data**

The change in viscosity was indicative of interactions having occurred between the reactants, to form a new molecule with a higher viscosity. *Bristle Density Calculations.* Taking the molecular weight of acrylic acid (monomer of PAA) as 72 Da, the number of binding sites on 1 mole PAA is ~3470. Theoretically, for a densely grafted brush, we would require at least 1 CS molecule for each binding site. Considering a PAA concentration of 10 mg/ml (Molarity  $4 \times 10^{-8}$  M), the equivalent molarity of acrylic acid is  $1.39 \times 10^{-4}$  M. The equivalent CS molarity to achieve a 1:1 molecule ratio is  $1.39 \times 10^{-4}$  M.

In our study, concentrations of CS and PAA used were 10 mg/ml each (Molarity CS:  $4.55 \times 10^{-7}$  M, PAA:  $4 \times 10^{-8}$  M), from which the CS:PAA mole ratio is 0.003, meaning there is 1 CS molecule for every 300 binding sites on PAA. This is a very low bristle density compared to the theoretical value calculated above. However, even a molarity as low as  $1.39 \times 10^{-4}$  M for CS results in the formation of a very viscous solution, which hinders its conjugation. Further investigation is required to modulate the CS concentration to achieve better bristle densities.

**Conclusions:** A biomimetic aggrecan polymer was successfully created and partially characterized for morphological and mechanical properties.

**References:** <sup>1</sup>Raj PP, *Pain Practice*, 8, 18-44, 2008, <sup>2</sup>Olczyk et al, *Zeitschrift für Rheumatologie* 1994;53(1):19-25, <sup>3</sup>Sarkar S et al. *SFB Annual Meeting 2010* Seattle, Washington, USA. We acknowledge C. Winkler (Drexel University) for TEM imaging and The Coulter Foundation for funding.