

Development of a Shape Memory Patch for Minimally Invasive Repair of Vascular Rupture

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Statement of Purpose: It is challenging and surgically risky to treat vascular injuries such as strokes and aneurysms, especially ruptures of small diameter blood vessels, through currently available therapeutic approaches. To address these issues, a vascular patch made of biodegradable shape memory polymers (SMPs) can be deployed to the injured or ruptured site in a minimally invasive manner via a laparoscope. SMPs are capable of achieving minimally invasive implantation and repair vascular injuries because they can be *fixed* into a temporary shape (i.e. an injectable shape for placement through a laparoscope) and *recover* their original, permanent shape (i.e. a ruptured tissue-specific shape) when triggered by an external stimulus such as heating above its melting temperature (T_m). Poly(ϵ -caprolactone) (PCL) is a biocompatible, biodegradable polymer that can be modified to form a chemically cross-linked polymer film with excellent shape memory properties¹. However, its T_m (45-60°C) is too high for physiological applications. In this study, the T_m was tuned near body temperature (37°C) by copolymerizing ϵ -caprolactone (CL) with α -allyl carboxylate- ϵ -caprolactone (ACCL). When polymerized, the pendant double bonds from the allyls enable formation of chemical cross-links that are essential for fixing and recovery of shape. UV cross-linking of $x\%$ PCL- $y\%$ ACPCL (x and y : molar ratio) produced polymer films with tunable shape memory properties, suggesting these novel SMPs offer promise in treating vascular injuries in a minimally-invasive way.

Methods: ACCL was first synthesized by adopting the method for α -benzyl carboxylate- ϵ -caprolactone². A series of $x\%$ PCL- $y\%$ ACPCL copolymers ($y = 6, 11, \text{ and } 15\%$) were synthesized by ring-opening polymerization of ACCL and CL. Polymers and 2,2-dimethoxy-2-phenylaceto-phenone were solubilized in dichloromethane and irradiated with a 260 nm UV collimated beam. Differential scanning calorimetry was performed to determine thermal properties³. Shape memory properties of cross-linked films were characterized on a TA Instruments Q800 dynamic mechanical analyzer (DMA). Rectangular strips (~20mm x ~3.0mm x ~0.3mm) were loaded onto a tension clamp and subjected to three of the following thermomechanical cycles. Equilibrated at $T_m + \sim 15^\circ\text{C}$, films were subjected to tensile stress (0.004 MPa/min to 0.039 MPa) as shown in (1) of Figure 1. Films were then cooled (10°C/min to 0°C) (2), yielding the strain at the maximum stress $\epsilon_1(N)$, before unloading the stress (0.004 MPa/min to 0 MPa) (3) and recording strain as $\epsilon_u(N)$, the temporary shape. Finally, the films were heated (2°C/min to $T_m + \sim 15^\circ\text{C}$) (4) to recover the permanent shape $\epsilon_p(N)$. The shape memory effect was quantified by shape fixity (R_f) and shape recovery (R_r). Shape fixity defines the ability to maintain a programmed shape induced by mechanical deformation, while shape recovery describes how well $\epsilon_p(N)$ is recovered from the beginning of the N^{th} cycle ($\epsilon_p(N-1)$):

$$R_f(N) = \frac{\epsilon_u(N)}{\epsilon_1(N)}; R_r(N) = \frac{\epsilon_p(N) - \epsilon_p(N-1)}{\epsilon_1(N) - \epsilon_p(N-1)}$$

Results: To successfully repair vascular tissue, SMPs should demonstrate a $T_m = \sim 37^\circ\text{C}$ with $R_f = \sim 100\%$ after mechanical deformation into an injectable shape. T_m 's of 44.6, 38.0, and 29.7°C for $y = 6, 11, \text{ and } 15\%$ copolymer films, respectively, suggest that shape recovery can be achieved in the body for $y = 11$ and 15% without the need for additional heating that could damage tissue and cause inconsistencies in shape recovery. All polymers demonstrated $R_f > 99\%$ after large (>30%) strains, indicating that the films can be programmed and fixed into a shape such as a long thread that can fit through a laparoscope. Furthermore, $R_r > 99\%$ was accomplished after repeated cycling, implying that a ruptured tissue-specific shape can be fully recovered if heated beyond the $T_m \sim 37^\circ\text{C}$.

Thermomechanical Cycling of PCL89-ACPCL11

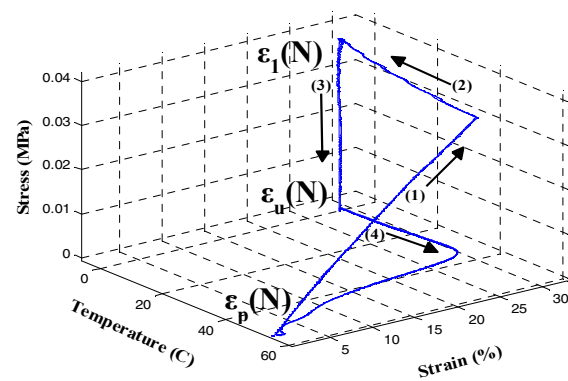


Figure 2. Initially at 0 MPa and 55°C , $y = 11\%$ was subjected to 0.004 MPa/min to 0.039 MPa (1), cooled (2), unloaded of tensile stress (3), and heated to recover shape (4). The cycle was repeated three times.

Conclusions: A new class of SMPs, PCL-ACPCL, was synthesized and characterized in order to develop a minimally invasive vascular patch for injuries of small diameter blood vessels to which proximal access is difficult (e.g., strokes). T_m 's near 37°C were achieved for 89%PCL-11%ACPCL and 85%PCL-15%ACPCL, indicating that shape recovery is possible for these polymers without implementing any risky heating procedures. Stress-controlled thermomechanical cycling demonstrated that these SMPs have an excellent ability to be programmed into an injectable shape for minimally invasive deployment to the site of injury as R_f was $>99\%$ for all films. R_r was also $>99\%$ after repeated cycling, suggesting these polymers can potentially assume a ruptured tissue-specific shape after implantation. PCL-ACPCL films will be tested in an *in vitro* vascular injury model.

References:

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- [3] Guo B. *Biomacromolecules* 2011;12:1312-1321.